Kidney Tumor Segmentation Based on U-Net and V-Net with Double Loss Function Training

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Abstract. Medical image processing plays an increasingly important role in clinical diagnosis and treatment. Using the results of kidney CT image segmentation for three-dimensional reconstruction is an intuitive and accurate method for diagnosis. However, the traditional image segmentation algorithm has poor performance due to the large difference of noise between kidney and CT images, and the manual segmentation by doctors will take a very long time and is inefficient. In this paper, we propose an in-depth learning automatic segmentation method for kidney tumors, including preprocessing of training data, network model used in training process, loss function and post-processing, etc. The results show that the average dice of kidney with tumor was 0.97 in the test set.

Keywords: Medical Image Segmentation, Deep Learning, Neural Network.

1 Introduction

Segmentation and reconstruction of CT or MRI medical images is the main source of navigation data, i.e. anatomical structure of tissues and organs[1-4]. At present, the most commonly used method of medical image segmentation is still manual segmentation, which takes a long time and depends on the operator's experience and skills[5]. In recent years, breakthroughs have been made in the research of neural networks[6-9]. The deep learning technology based on neural networks can achieve fast segmentation, and effectively solve the problem of low accuracy and long time-consuming image segmentation[10]. In the field of medical image segmentation, the break-through of in-depth learning began with the introduction of Full Convolutional Neural Network (FCN), and another breakthrough of neural network architecture U-Net made it possible to achieve high-precision automatic segmentation of medical images. Long Jonathan et al.[11]

In this paper, we propose an in-depth learning automatic segmentation method for kidney tumors, including preprocessing of training data, network model used in training process, loss function and post-processing, etc.

2 Operational Process

2.1 Initial Segmentation Using U-NET

Firstly, we divide the data set into two parts: 200 patients' CT sequences as training sets and 10 patients' CT sequences as test sets. Then we use the training set to train U-NET directly for segmentation task, which is to roughly find the region of kidney. Figure 1 shows the results of segmentation, in which the results of segmentation have met our expectations.

As in (1), we use Binary Cross Entropy(BCE)[12] to measure the error between model output and label in medical image processing.

$$loss(o,t) = -\frac{1}{n} \sum_{i=0}^{n} (t[i]log(o[i]) + (1 - t[i])log(1 - o[i]))$$
(1)



Fig. 1. The result of initial segmentation

2.2 Fine Segmentation Using V-NET

In this step, we will use the results of the previous step to calculate the area of the kidney and tailor it. As shown in Figure 2, we cut the mask part into a threedimensional sequence. In order to generate trainset for V-Net, we scale this threedimensional sequence to 128*128*64 sequence. Then we use the segmentation result of training set to train V-Net to segment kidney and tumor. It is worth noting that during the training process, we tested several different loss functions and functions defined by ourselves to test the effect. Including weight cross-entropy, square deviation and Dice loss function. The results show that the square difference and Dice loss function are more suitable for the task of three-dimensional segmentation. At this stage, we still use the CT sequences of the first 200 patients as training set. After cutting, we obtained 390 sequences of 128*128*64 containing kidneys.

2



Fig. 2. The result of fine segmentation

2.3 Restoring to Original CT Part

After the first two steps, we can get a U-Net model which can segment the kidney from 512*512 image, a 128*128*64 three-dimensional sequence cut and scaled according to the U-Net result, a V-Net model which can segment the kidney from 128*128*64 three-dimensional sequence, and a segmented and deformed kidney in 128*128*64 sequence. In this step, we restore the segmentation result to the original CT image size. As shown in Figure 3, by comparison, it can be found that the segmentation results obtained by this method are better than direct segmentation in most cases.



Fig. 3. Comparison of segmentation results. (a)CT image. (b)result of U-Net. (c)result of V-Net.

2.4 Kidney Tumor Segmentation Model Training

The V-Net model is also trained for the segmentation of kidney tumors. As in the second step, we regard the tumors as another label of 128*128*64 sequence. The segmentation results of the model are restored to the original size by the same restoring method as in the third step.

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4